Modelling of Orthogonal Craniofacial Profiles

Hang Dai 1,*, Nick Pears 1 and Christian Duncan 2

1 Department of Computer Science, University of York, Heslington, York YO10 5GH, UK; nick.pears@york.ac.uk
2 Alder Hey Children’s Hospital, Liverpool L12 2AP, UK; Christian.Duncan@alderhey.nhs.uk
* Correspondence: hd816@york.ac.uk; Tel.: +44-1904-325-643

Received: 20 October 2017; Accepted: 23 November 2017; Published: 30 November 2017

Abstract: We present a fully-automatic image processing pipeline to build a set of 2D morphable models of three craniofacial profiles from orthogonal viewpoints, side view, front view and top view, using a set of 3D head surface images. Subjects in this dataset wear a close-fitting latex cap to reveal the overall skull shape. Texture-based 3D pose normalization and facial landmarking are applied to extract the profiles from 3D raw scans. Fully-automatic profile annotation, subdivision and registration methods are used to establish dense correspondence among sagittal profiles. The collection of sagittal profiles in dense correspondence are scaled and aligned using Generalised Procrustes Analysis (GPA), before applying principal component analysis to generate a morphable model. Additionally, we propose a new alternative alignment called the Ellipse Centre Nasion (ECN) method. Our model is used in a case study of craniosynostosis intervention outcome evaluation, and the evaluation reveals that the proposed model achieves state-of-the-art results. We make publicly available both the morphable models and the profile dataset used to construct it.

Keywords: morphable model; shape modelling; craniofacial; craniosynostosis

1. Introduction

In the medical analysis of craniofacial shape, the visualisation of 2D profiles [1] is highly informative when looking for deviations from population norms. It is often useful, in terms of visual clarity and attention focus, for the clinician to examine shape outlines from canonical viewpoints; for example, pre- and post-operative canonical profiles can be overlaid. We view profile-based modelling and analyses as being complementary to that of a full 3D shape model. Profile visualisations should be backed up by quantitative analysis, such as the distance (in standard deviations) of a patient’s shape profile from the mean profile of a reference population. Therefore, we have developed a novel image processing pipeline to generate a 2D morphable model of craniofacial profiles from a set of 3D head surface images. We construct morphable 2D profile models over three orthogonal planes to provide comprehensive models and analyses of shape outline.

A morphable model is constructed by performing some form of dimensionality reduction, typically Principal Component Analysis (PCA), on a training dataset of shape examples. This is feasible only if each shape is first re-parametrised into a consistent form where the number of points and their anatomical locations are made consistent to some level of accuracy. Shapes satisfying these properties are said to be in dense correspondence with one another. Once built, the morphable model provides two functions. Firstly, it is a powerful prior on 2D profile shapes that can be leveraged in fitting algorithms to reconstruct accurate and complete 2D representations of profiles. Secondly, the proposed model provides a mechanism to encode any 2D profile in a low dimensional feature space; a compact representation that makes tractable many 2D profile analysis problems in the medical domain.

Contributions: We propose a new pipeline to build a 2D morphable model of the craniofacial sagittal profile and augment it with profile models from frontal and top down views. We also integrate
all three profiles into a single model, thus capturing any correlations within and between the three profile shapes more explicitly and clearly than is possible with PCA analysis on a full 3D model. A new pose normalisation scheme is presented called Ellipse Centre Nasion (ECN) normalisation. Extensive qualitative and quantitative evaluations reveal that the proposed normalisation achieves state-of-the-art results. We use our morphable model to perform craniosynostosis intervention outcome evaluation on a set of 25 craniosynostosis patients. For the benefit of the research community, we will make publicly available (on email request to the first author) the three profile datasets over a 1212-subject dataset; all of our 2D morphable models will be downloadable with MATLAB GUI code to view and manipulate the models.

Paper structure: In the following section, we discuss related literature. Section 3 discusses our new pipeline used to extract profiles and construct 2D morphable models. The next section evaluates several variants of the constructed models both qualitatively and quantitatively, while Section 5 compares our single-view models with our multi-view model. Section 6 illustrates the use of the morphable model in intervention outcome assessment for a population of 25 craniosynostosis patients. A final section concludes the work.

2. Related Work

In the late 1990s, Blanz and Vetter built a ‘3D Morphable Model’ (3DMM) from 3D face scans [2] and employed it in a 2D face recognition application [3]. Two hundred scans were employed (young adults, 100 males and 100 females). Dense correspondences were computed using a gradient-based optic flow algorithm; both shape and colour-texture are used. The model is constructed by applying PCA to shape and colour-texture (separately).

The Basel Face Model (BFM) is the most well-known and widely-used face model and was developed by Paysan et al. [4]. Again, 200 scans were used, but the method of determining corresponding points was improved. Instead of optic flow, a set of hand-labelled feature points is marked on each of the 200 training scans. The corresponding points are known on a template mesh, which is then morphed onto the training scan using underconstrained per-vertex affine transformations, which are constrained by regularisation across neighbouring points [5]. Recently, a similar morphing strategy was used to build a facial 3DMM from a much larger dataset (almost 10,000 faces) [6], although there is no cranial shape information in the model.

The Iterative Closest Points (ICP) algorithm [7,8] is the basic method to address the point registration problem. Several extensions of ICP for the non-rigid case were proposed [5,9–13]. Other deformable template methods could be used to build morphable models [14,15], such as Thin Plate Splines (TPS) [16], TPS with Robust Point Matching (TPS-RPM) [17], the non-rigid point and normal registration algorithm of Lee et al. [18], relaxation labelling [19] or the manifold learning method of Ma et al. [20]. The global correspondence optimization method solves simultaneously for both deformation parameters, as well as the correspondence positions [21]. Myronenko et al. consider the alignment of two point sets as a probability density estimation [22], and they call the method Coherent Point Drift (CPD); this remains a highly competitive template morphing algorithm.

Template morphing methods need an automatic initialisation to bring them within the convergence basin of the global minimum of alignment and morphing. To this end, Active Appearance Models (AAMs) [23] and elastic graph matching [24] are the classic approaches of facial landmark and pose estimation. Many improvements over AAM have been proposed [25,26]. Recent work has focused on global spatial models built on top of local part detectors, sometimes known as Constrained Local Models (CLMs) [27,28]. Zhu and Ramanan [29] use a tree structured part model of the face, which both detects faces and locates facial landmarks. One of the major advantages of their approach is that it can handle extreme head pose.

Another relevant model-building technique is the Minimum Description Length method (MDL) [30], which selects the set of parameterizations that build the ‘best’ model, where ‘best’ is defined as that which minimizes the description length of the training set.
3. Model Construction Pipeline

Our pipeline to build a 2D morphable model is illustrated in Figure 1. Input data (left of figure) consists of 1212 3D images of subjects with an even split of males and females. This is a subset of the Headspace dataset, captured using 3dMD’s 5-camera 3dMDhead system. All subjects are wearing tight-fitting latex caps to expose the shape of the cranium, and we excluded around 300 scans from the dataset, primarily due to visible hair bulges or poor fitting of the cap. The processing pipeline in Figure 1 employs a range of techniques in both 3D surface image analysis and 2D image analysis and has three main stages:

(i) 2D shape extraction: The raw 3D scan from the Headspace dataset undergoes pose normalization and preprocessing to remove redundant data (lower neck and shoulder area), and the 2D profile shape is extracted as closed contours from three orthogonal viewpoints: the side view, top view and frontal view (note that we automatically remove the ears in the top and frontal views, as it is difficult to get good correspondences over this section of the profiles).

(ii) Dense correspondence establishment: A collection of profiles from a given viewpoint is reparametrised into a form where each profile has the same number of points joined into a connectivity that is shared across all profiles.

(iii) Similarity alignment and statistical modelling: The collection of profiles in dense correspondence are subjected to Generalised Procrustes Analysis (GPA) to remove similarity effects (rotation, translation and scale), leaving only shape information. The processed meshes are statistically analysed, typically with PCA, generating a 2D morphable model expressed using a linear basis of eigen shapes. This allows for the generation of novel shape instances, over any of the three viewpoints.

Figure 1. The pipeline for 2D morphable model construction. Note that 2D profiles are extracted as closed contours from three orthogonal viewpoints.

Each of the profiles is represented by \( m \) 2D points \((y_i, z_i)\) and is reshaped to a \( 2m \) row vector. Each of these vectors is then stacked in a \( n \times 2m \) data matrix, and each column is made zero mean. Singular Value Decomposition (SVD) is applied from which eigenvectors are given directly and eigenvalues can be computed from singular values. This yields a linear model as:

\[
x_i = \bar{x} + Pb_i = \bar{x} + \sum_{i=1}^{k} p^k b^k_i
\]

where \( \bar{x} \) is the mean head profile shape vector and \( P \) is a matrix whose columns \( p^k \) are the eigenvectors of the covariance matrix (after pose alignment), describing orthogonal modes of head profile variation. The vector \( b \) holds the shape parameters \( \{b^k\} \) that weight the shape variation modes, which when added to the mean shape, model a shape instance \( x_i \). The three main stages of the pipeline are described in the following subsections.
3.1. 2D Shape Extraction

2D shape extraction requires three stages, namely (i) pose normalisation, (ii) cropping and (iii) edge detection. Each of these stages is described in the following subsection.

3.1.1. Pose Normalisation

Using the colour-texture information associated with the 3D mesh, we can generate a realistic 2D synthetic image from any view angle. We rotate the scan over 360 degrees in pitch and yaw (10 steps of each) to generate 100 images. Then, the Viola–Jones face detection algorithm [31] is used to find the frontal face image among this image sequence. A score is computed that indicates how frontal the pose is. The 2D image with the highest score is chosen to undergo 2D facial landmarking. We employ the method of Constrained Local Models (CLMs) using robust discriminative response map fitting [32] to do the 2D facial image landmarking. Then, the trained system is used to estimate the three angles for the image with facial landmarks. Finally, 3D facial landmarks are captured by projecting the 2D facial landmarks to the 3D scan. As shown in Figure 2, by estimating the rigid transformation matrix $T$ from the landmarks of a 3D scan to that of a template, a small adjustment of pose normalization is implemented by transforming the 3D scan using $T^{-1}$.

![Figure 2. 3D pose normalization using the texture information.](image)

3.1.2. Cropping

3D facial landmarks can be used to crop out redundant points, such as the shoulder area and long hair. The face landmarks delineate the face size and its lower bounds on the pose normalised scan, allowing any of several cropping heuristics to be used. We calculate the face size by computing the average distance from facial landmarks to their centroid. Subsequently, a plane for cropping the 3D scan is generated by moving the cropping plane downward an empirical percentage of the face size. We use a sloping cropping plane so that the chin area is included, but that still allows us to crop close to the base of the latex skull cap at the back of the neck to remove the (typically noisy) scan region, where the subject’s hair emerges from under the cap (see Figure 1).

3.1.3. Edge Detection

We use side view, top view and frontal view from the 3D scan to reveal the 2D profile shape, and we can generate a 2D contour within the three views by orthogonal projection. For example, in the side view (Y-Z view), we traverse the Y direction in small steps, and at each step, we compute the minimum and maximum Z value. The points with the minimum and maximum Z value are the contour points in the side view.
3.1.4. Automatic Annotation

A machine learning method of finding approximate facial landmark localisations was described in Section 3.1.1. The \((y, z)\) positions of these landmarks are used to indicate the approximate locations of landmarks on the extracted profile, by closest point projection. These can be considered as initial approximate landmark positions, which then can be refined by a local optimisation, based on a disc operator applied to the local structure of the profile. In this method, we centre a disc (at the largest scale that we are interested in) on some point on the head profile and fit, by least squares, a quartic polynomial to the profile points within that disc. A quartic was chosen to give the flexibility to fit to the ‘double peaked’ area over the lips. Thus, we find quartic parameters \(p^T\) to fit a set of profile points \([x_p, y_p]\) such that, with \(n = 4\):

\[
y_p = p^T x_p, \quad p = [p_0 \ldots p_n]^T, \quad x_p = [x_p^0 \ldots x_p^n]^T
\]  

To implement our disc operator, we take a dense, regularly-spaced set of \(n\) point samples within that disc, \([x_d, y_d]\) and compute the operator value as:

\[
\alpha = \frac{1}{n} \sum_{i=1}^{n} \text{sign}(y_d - p^T x_d)
\]  

We find that \((-1 \leq \alpha \leq 1)\), with values close to zero indicating locally flat regions, positive values indicating convexities, such as the pronasale (nose tip), and negative values indicating concavities, such as the nasion. Effectively, this is a discrete approximation to finding the area within the facial profile that intersects with a disc of some predefined scale. The discrete sampling gives a high frequency quantisation noise on the signal, and so, we filter this with a 10th order low pass Butterworth filter.

The operator is very easily adapted to multiple scales, with smaller scales being straightforward subsamples of the disc points \([x_d, y_d]\) at larger scales. In this case, we reapply Equation (3) to the subsample and, as with the larger scale, apply a low pass filter. A useful property of the operator, in contrast to a standard curvature operator, is that its scale is easily tuned to the size of the features that one is interested in: we use a 20-mm disc radius for most profile landmarks (nasion, pronasale, subnasale, chin concavity and pogonion), except those around the lips (upper lip, lower lips, centre of lips), where we use the smallest scale, 5 mm. Figure 3 illustrates the disc operator’s output at four scales to illustrate its behaviour. For five of eight facial profile landmarks, the strongest output is (usually) the largest scale. For the remaining three, the strongest output is the smallest scale.

The landmarking algorithm employed finds the nearest strong local extrema of the appropriate sign and at the appropriate scale. We first refine the pogonion (chin), subnasale, pronasale (nose tip) and nasion at the largest operator scale. We then consider upper, centre and lower lips simultaneously by looking for a strong M-shaped disc operator signature at the smallest scale (5 mm, cyan, in Figure 3), between the subnasale and pogonion. Finally, we find the chin cleft location as the strongest minimum between the lower lip and pogonion.

3.2. Correspondence Establishment

To extract profile points using subdivision, we have an interpolation procedure that ensures that there is a fixed number of evenly-spaced points between any pair of facial profile landmarks. However, it is not possible to landmark the cranial region and extract profile model points in the same way. This area is smooth and approximately elliptical in structure, and so, we project vectors from the ellipse centre and intersect a set of fitted cubic spline curves, starting at the nasion and incrementing the angle anticlockwise in small steps (we use one degree) over a fixed angle.
Figure 3. (a) Automatic (red cross) and manual (cyan circle) landmarks on a facial profile. (b) The disc operator output at multiple scales, with landmark positions at the signal’s extrema. Red = 20 mm radius, green = 15 mm, blue = 10 mm, cyan = 5 mm radius. Landmarks are located at the strongest scale, which is different for differently-sized features.

As well as using subdivision points directly in model construction, we form a model template as the mean of the population of subdivided and aligned profiles, and we use template deformation on the dataset. The resulting deformed templates are re-parametrised versions of each subject that are in correspondence with one another. In this paper, we apply subdivision, Thin Plate Splines (TPS) [16], Non-rigid Iterative Closest Points (NICP) [5], Li’s method [21], Coherent Point Drift (CPD) [22] and Minimum Description Length (MDL) [30] to the proposed pipeline for comparative performance evaluation.

3.3. Similarity Alignment

A profile alignment method is needed before PCA can be applied to build the 2DMM. We use both the standard GPA approach and a new Ellipse Centre Nasion (ECN) method. Ellipse fitting was motivated by the fact that large sections of the cranium appeared to be elliptical in form, thus suggesting a natural centre and frame origin with which to model cranial shape. One might ask: Why not just use GPA over the whole head for alignment? One reason is because variable facial feature sizes (e.g., the nose or chin’s Pinocchio effect) induce displacements in the cranial alignment, which is a disadvantage if we are primarily interested in cranial rather than facial shape. We use the nasion’s position to segment out the cranium region from the face and use a robust iterative ellipse fitting procedure that rejects outliers.

Figure 4 shows examples of the robust ellipse fit for two head profiles. The centre of the ellipse is used in a pose normalisation procedure where the ellipse centre is used as the origin of the profile and the angle from the ellipse centre to the nasion is fixed at −10 degrees. We call this Ellipse Centre Nasion (ECN) pose normalisation and later compare this to GPA. The major and minor axes of the extracted ellipses are plotted as red and green lines respectively in Figure 4.
Figure 4. Head tilt pose normalisation (a,b) based on Ellipse Centre and Nasion (ECN) position. The extracted head profile is shown in blue; red crosses show facial landmarks; and the ellipse fitted to the cranial profile is shown in cyan. Its major axis is red, and its minor axis green. Reproduced with permission [1].

Figure 5 shows all the profiles overlaid with the same alignment scheme. We noted regularity in the orientation of the fitted ellipse as is indicated by the clustering of the major (red) and minor (green) axes in Figure 5 and the histogram of ellipse orientations in Figure 5. A minority of heads (9%) in the training sample have their major ellipse axes closer to the vertical (brachycephalic).

Figure 5. (a) All training profiles after ECN normalisation; (b) major axis ellipse angles with respect to an ECN baseline of −10 degrees: median angle is −6.4 degrees (2sf). Reproduced with permission [1].

4. Morphable Model Evaluation

We built four 2DMM variants of the side-view profile using 100 males from the Headspace dataset and animated shape variation along the principal components (later, the full dataset is used). The four model variations correspond to full head, scale normalised and unscaled, and cranium only, scale normalised and unscaled.

As an example, when ECN is used (Figure 6, first row), the following three dominant (unscaled) modes are observed: (i) cranial height with facial angle are the main shape variations, with small cranial heights being correlated with a depression in the region of the coronal suture; (ii) the overall size of the head varies; surprisingly, this appears to be almost uncorrelated with craniofacial profile
shape; this was only found in the ECN method of pose normalisation; (iii) the length of the face varies; i.e., there is variation in the ratio of face and cranium size. The second row of Figure 6 shows the model variation using GPA alignment for comparison.

Figure 6. (a) The dominant three modes (left: Mode 1; centre: Mode 2; right: Mode 3) of head shape variation using automatic profile landmark refinement and ECN similarity alignment. The mean is blue, mean + 3 SD is red; and mean – 3 SD is green. (b) Generalised Procrustes Analysis (GPA) similarity alignment. Reproduced with permission [1].

For quantitative evaluation of morphable models, Styner et al. [33] give detailed descriptions of three metrics: compactness, generalisation and specificity, now used on our scale-normalised models.

Compactness: This describes the number of parameters (fewer is better) required to express some fraction of the variance in the training set. As illustrated in Figure 7, the compactness using ECN alignment is superior to that of GPA alignment, for all correspondence methods. Among these correspondence methods, subdivision, TPS and MDL, all aligned with ECN, are able to generate the most compact models.

Specificity: Specificity measures the model’s ability to generate shape instances of the class that are similar to those in the training set. We generate 1000 random samples and take the average Euclidean distance error to the closest training shape for evaluation; lower is better. We show the specificity error as a function of the number of parameters in Figure 8. Across all correspondence methods with GPA, it gives better specificity against all correspondence methods with ECN. This suggests that GPA helps improve the performance of modelling the underlying shape space. NICP with GPA capture the best specificity.

Generalisation: Generalisation measures the capability of the model to represent unseen examples of the class of objects. It can be measured using the leave-one-out strategy, where one example is omitted from the training set and used for reconstruction testing. The accuracy of describing the unseen example is calculated by the mean point-to-point Euclidean distance error; the lower the better. Generalization results are shown in Figure 8, and for more parameters, the error decreases, as expected. NICP with GPA performs better in terms of Euclidean distance once less than seven model dimensions are used. Between seven and 20 model dimensions, TPS with ECN outperforms other methods. When more than 20 model dimensions are used, CPD with GPA has the best generalization ability. Overall, GPA is able to help more successfully model the underlying shape against ECN for the same correspondence method, thereby generating better reconstructions of unseen examples.
Figure 7. Compactness (a, b); higher is better. The right figure is used to zoom into where the differences between the methods is greatest. Alignment methods: ECN, Ellipse Centre Nasion; GPA, Generalised Procrustes Analysis. Correspondence methods: Subdiv, Subdivision; TPS, Thin Plate Splines; NICP, Non-rigid Iterative Closest Points; Li, Li’s method [21]; CPD, Coherent Point Drift; MDL, Minimum Description Length. Please view in colour to distinguish the plots. Reproduced with permission [1].

Figure 8. (a) specificity; (b) generalization. A lower error is better for both metrics. Alignment methods: ECN, GPA. Correspondence methods: Subdiv, TPS, NICP, Li [21], CPD, MDL. Please view in colour to distinguish the plots. Reproduced with permission [1].

5. Single-View Models versus the Global Multi-View Model

We used the proposed pipeline to build three separate viewpoint 2DMM profile models with GPA and PCA with over 1212 subjects and an even split of males and females. The variations of the four main modes are shown in Figure 9. These models can be used for the analysis of 2D shape from the profile, the side, top and frontal view, respectively. However, clearly, the the three views are correlated with each other, and constructing a global model comprising all three views allows us to analyse this correlation. In order to do that, we put the 2D shape back to 3D within the respective orthogonal planes, as shown in Figure 10. In X-Y-Z frames, the global similarity can be removed by GPA, and the correlation among the three views can be revealed by PCA. Four modes from the global model are illustrated in Figure 11. Obviously, the variations in Y-Z, X-Z and X-Y within the global model are different from those variations in the separate models in Figure 9.
To validate the effectiveness of the global model, we use the parameters from the morphable model to do age and gender classification in the Headspace dataset over 1212 subjects. Using the demographic information (metadata) within the dataset we train a Support Vector Machine (SVM) classifier for each model, which maps the corresponding shape vectors to the gender groups and four age groups (0–11, 12–21, 22–60 and over 60). To measure the classification accuracy, we use the classifier to predict the age bracket and the gender for the test subjects via a 10-fold cross-validation evaluation so that no test subject ever appears in the classifier’s training set. As can be seen in Tables 1 and 2, the global model has the best performance in both gender and age classification, and the side
profile is slightly stronger than the other two separate profiles, as may be expected from the larger curvature variability within that profile.

Figure 11. Global model, showing the first four modes (a–d) of shape variation.

Table 1. Gender classification.

<table>
<thead>
<tr>
<th>Models</th>
<th>Precision</th>
<th>Recall</th>
<th>F-score</th>
</tr>
</thead>
<tbody>
<tr>
<td>Top</td>
<td>0.64</td>
<td>0.65</td>
<td>0.64</td>
</tr>
<tr>
<td>Frontal</td>
<td>0.73</td>
<td>0.73</td>
<td>0.73</td>
</tr>
<tr>
<td>Profile</td>
<td>0.77</td>
<td>0.77</td>
<td>0.77</td>
</tr>
<tr>
<td>Global</td>
<td>0.79</td>
<td>0.79</td>
<td>0.79</td>
</tr>
</tbody>
</table>

Table 2. Age classification.

<table>
<thead>
<tr>
<th>Models</th>
<th>Precision</th>
<th>Recall</th>
<th>F-score</th>
</tr>
</thead>
<tbody>
<tr>
<td>Top</td>
<td>0.72</td>
<td>0.72</td>
<td>0.72</td>
</tr>
<tr>
<td>Frontal</td>
<td>0.71</td>
<td>0.71</td>
<td>0.71</td>
</tr>
<tr>
<td>Profile</td>
<td>0.73</td>
<td>0.73</td>
<td>0.73</td>
</tr>
<tr>
<td>Global</td>
<td>0.75</td>
<td>0.76</td>
<td>0.75</td>
</tr>
</tbody>
</table>

6. Craniosynostosis Intervention Outcome Evaluation

Craniosynostosis is a skull condition whereby, during skull growth and development, the sutures prematurely fuse, leading to both an abnormally-shaped cranium and increased intracranial...
We present a case study of 25 craniosynostosis patients (all boys), 14 of which have undergone one type of corrective procedure called Barrel Staving (BS) and the other 11, another corrective procedure called Total Calvarial Remodelling (TCR). The intervention aim is to remodel the patient’s skull shape towards that of an adult, and we can employ our model in assessing this.

We build a scale-normalised, cranium only (to the nasion) 2D morphable model (2DMM) using 100 male subjects, without cranial conditions. Given that the model is to be used to assess surgical remodelling of the cranial shape (and not the face), we build a model of the cranial part only. We also scale normalise for better alignment of training data and to factor out patient growth between pre- and post-operative scans. We note also that major cranial shape changes are not thought to occur after two years old. The patients’ scale-normalised profiles are then parametrised using the model, indicating the distance from the mean cranial shape in terms of the model’s eigenstructure. The comparisons of pre-operative and post-operative parametrisations show the shapes moving nearer to the mean of the training examples; see Figure 12.

For the BS patient set, the Mahalanobis distance of the mean pre-op parameters (red triangle in Figure 12) is 4.670 and for the mean post-op parameters (blue triangle) is 2.302. For Shape Parameter 2 only (the dominant effect), these figures are 4.400 and 2.156. For the TCR patient set, the Mahalanobis distance of the mean pre-op parameters (red triangle in Figure 12) is 4.647 and for the mean post-op parameters (blue triangle) is 2.439. For Shape Parameter 2 only, these figures are 4.354 and 2.439. We note that most of this change occurs in Parameter 2, which corresponds to moving height in the cranium from the frontal part of the profile to the rear. In these figures, we excluded one patient, who preoperatively already had a near-mean head shape (see the red cross near the origin in Figure 12), so any operation is unlikely to improve on this (but intervention is required in order to relieve potentially damaging intracranial pressure).

It is not possible to make definitive statements relating to one method of intervention compared to another with these relatively small numbers of patients. However, the cranial profile model does show that both procedures on average lead to a movement of head shape towards the mean of the training population. Examples of the analysis of the intervention outcome for a BS patient and a TCR patient are given in Figure 13. The particular example used is highlighted with circles in Figure 12 to indicate pre-op and post-op parametrisations.
Figure 13. (a) Pre-op and post-op profiles for a BS patient; (b) Pre-op and post-op profiles for a TCR patient. The red and blue traces show the extracted sagittal profiles of the patient pre-operatively and post-operatively, respectively, whilst the green shows the mean profile of the training set. Reproduced with permission [1].

7. Conclusions

We have presented a fully-automatic, general and powerful head profile modelling pipeline that can extract 2D profiles from three orthogonal planes and build both separate and global (combined) morphable models of these profiles. We have thoroughly evaluated two profile alignment methods and six correspondence methods, giving twelve possible model-building systems enabling the research community to compare and contrast performance across these variants using three different metrics: compactness, specificity and generalisation. We make our profile models and the data employed to build them publicly available for the research community, enabling others to build models with their own algorithms and compare them to ours. We have shown that the models can be used to build software tools that aid the assessment of craniofacial surgery via a case study involving 25 craniosynostosis patients.

Acknowledgments: We thank Google Faculty Awards, the Royal Academy of Engineering and the Leverhulme Trust for their support. Headspace data collection was supported by Quality Improvement, Development and Innovation (QIDIS). We also thank Rachel Armstrong, Headspace project coordinator.

Author Contributions: Hang Dai contributed 50% to the shape modelling concepts and algorithms, he did the majority of the code design and implementation, he designed and implemented all of the evaluations, and wrote the first draft of the paper. Nick Pears contributed 50% to the shape modelling concepts and algorithms, he contributed to the code design and implementation, he directed the project, and revised the paper. Christian Duncan directed the data collection process and provided clinical advice on the medical evaluation experiments.

Conflicts of Interest: The authors declare no conflict of interest. The founding sponsors had no role in the design of the study; in the collection, analyses or interpretation of data; in the writing of the manuscript; nor in the decision to publish the results.
References


© 2017 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (http://creativecommons.org/licenses/by/4.0/).